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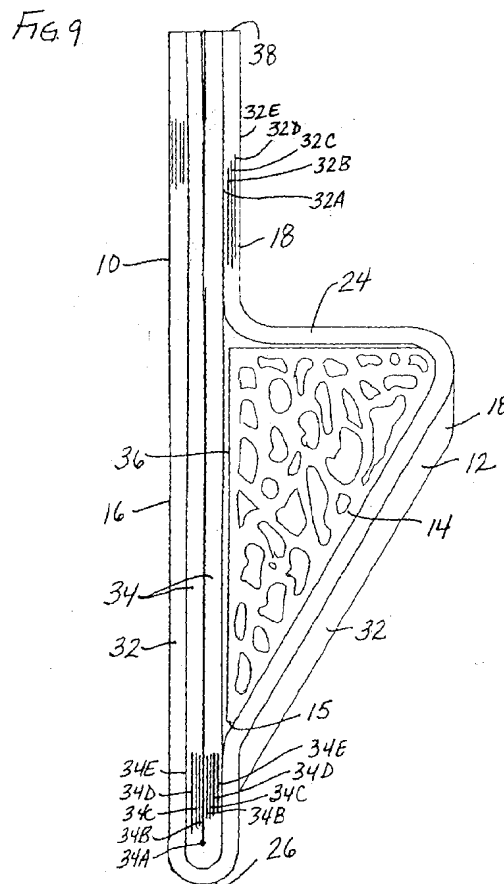
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(54) **Implantable tissue repair device**

(57) An implantable tissue repair device has a cover and tissue regeneration material. The cover includes a top panel and a bottom panel joined together along a leading edge. The tissue regeneration material is positioned between the top and bottom panels. The cover includes a continuous sheet of biocompatible material extending across the edge and into the top panel and bottom panel. The cover is thicker along the leading edge than at least a portion of the top panel and thicker than at least a portion of the bottom panel. At least a portion of one of the panels covering the tissue regeneration material is thicker than a portion of the other panel covering the tissue regeneration material.



Description

[0001] The present invention relates generally to surgical devices or implants for repairing and regenerating damaged or diseased fibrocartilage, and to a method of making such devices.

[0002] Articular cartilage is a type of hyaline cartilage that lines the surfaces of the opposing bones in a diarthrodial joint (e.g. knee, hip, shoulder, etc.). Articular cartilage provides a near frictionless articulation between the bones, while also functioning to absorb and transmit the compressive and shear forces encountered in the joint. Further, since the tissue associated with articular cartilage is aneural, these load absorbing and transmitting functions occur in a painless fashion in a healthy joint.

[0003] Human joints also have another type of cartilage present: intra-articular fibrocartilage. Intra-articular fibrocartilage can be present in the form of a discus articularis, that is, as a plate or ring of fibrocartilage in the joint capsule separating the joint surfaces (articular cartilage) of the bones of the joint. Such fibrocartilage is present, for example, in the temporomandibular joint, between vertebrae, and in the knee joint. In the knee joint, the intra-articular fibrocartilage comprises the meniscus, a crescent-shaped or semi-lunar-shaped disc of tissue that is located between the femoral condyles and the tibial plateau. The meniscus primarily functions as a shock absorber, absorbing the shock of compressive and shear forces in the knee. The meniscus also provides a substantially frictionless surface for articulation of the knee joint.

[0004] When cartilage tissue is no longer healthy, there can be debilitating pain in the joint. Cartilage health can be adversely affected by disease, aging, or trauma. The adverse effects of disease, aging and trauma can be in the form of a tear in the cartilage or in the form of a breakdown of the cartilage matrix.

[0005] In the knee, the meniscus is frequently damaged in twisting injuries. It is also damaged with repetitive impact over time. Meniscus degeneration can also occur by aging; as a person ages, the meniscus can become soft in places, so that even common motions like squatting can cause meniscal tears. Such degenerative or traumatic tears to the meniscus, which result in partial or complete loss of function, frequently occur in the white-white zone of the meniscus. Such tears result in unstable flaps of meniscal tissue in the knee joint causing, in the short term, severe joint pain and locking, and in the long term, a loss of mechanical function leading to osteoarthritis.

[0006] Common surgical procedures for treating meniscal damage include tear repairs and menisectomies. A tear repair is most commonly performed when the tear is a clean longitudinal vertical lesion in the vascular red zone of the meniscus. The basic strategy is to stabilize the tear by limiting or eliminating radial separation of the faces of the tear when the meniscus is load bearing.

Many devices and surgical procedures exist for repairing meniscal tears by approximating the faces of the meniscus at the tear. Examples of such devices and procedures are disclosed in US-6319271, US-6306159, US-6306156, US-6293961, US-6156044, US-6152935, US-6056778, US-5993475, US-5980524, US-5702462, US-5569252, US-5374268, US-5320633, and US-4873976.

[0007] Menisectomies involve the surgical removal of part of the meniscus. Such procedures have generally been performed in cases of radial tears, horizontal tears, vertical longitudinal tears outside the vascular zone, complex tears, or defibrillation. Although menisectomies provide immediate relief to the patient, in the long term the absence of part of the meniscus can cause cartilage wear on the condylar surface, eventually leading to arthritic conditions in the joint. And when the resected tissue is from the avascular, white-white zone, the meniscus has little potential for self-regeneration. Thus, removal of meniscal tissue from the avascular white-white zone can result in partial or permanent loss of meniscal tissue, making the joint susceptible to osteoarthritis.

[0008] Attempts have been made to regenerate meniscal tissue following a menisectomy. Previous attempts have included the use of surgical techniques and implants. The surgical techniques have been used to provide vascularity to the avascular region through synovial abrasion or by providing vascular access channels. Implants have included fibrin clot, meniscal allografts (see Stollsteimer, G.T., et al., "Meniscal allograft transplantation: a 1-to 5-year follow-up of 22 patients," *Arthroscopy*, 16(4): pp 343-7 (2000); Rodeo, S.A., "Meniscal allografts--where do we stand," *Am J Sports Med*, 29(2): pp. 246-61 (2001)), synthetic biodegradable polymer implants (with or without cells), a collagen scaffold device made at least in part from purified natural fibres that are cross-linked to form the device and scaffolds made from synthetic polymers.

[0009] A scaffold device made from purified collagen is described in US-6042610. A meniscal augmentation device for a damaged meniscus is also disclosed in US-5735903, US-5681353, US-5306311, US-5108438, US-5007934 and US-4880429.

[0010] A scaffold device made from a synthetic polymer is described by Klompmaker, J., et al. in "Meniscal replacement using a porous polymer prosthesis: a preliminary study in the dog," *Biomaterials*, 17(2): pp 1169-75 (1996) and by deGroot, J.H., et al., "Use of porous polyurethanes for meniscal reconstruction and meniscal prostheses," *Biomaterials*, 17(2): pp. 163-73 (1996). Medical applications for synthetic polymers are also disclosed in documents such as US-6224892, US-5847012 and US-5677355.

[0011] The previous attempts at regenerating meniscal tissue have been problematic. While providing vascularity at the site of meniscal lesions may work well for more stable meniscal tears where very little tissue has been lost, providing vascularity where there is signifi-

cant tissue loss (for example, due to meniscectomy) has not consistently resulted in an acceptable outcome. See Arnoczky, S.P. and R.F. Warren, "The microvasculature of the meniscus and its response to injury. An experimental study in the dog, *Am J Sports Med*, 11(3): p. 131-41 (1983); Fox, J. M., K.G. Rintz. and R.D. Ferkel, "Trephination of incomplete meniscal tears," *Arthroscopy*, 9(4): p. 451-5 (1993). Although autologous fibrin clot can be effective in regenerating critical sized defects, Arnoczky, S.P., R.F. Warren, and J. M. Spivak, "Meniscal repair using an exogenous fibrin clot. An experimental study in dogs," *J Bone Joint Surg Am*, 70(8):pp1209-17 (1988). The fragility of a fibrin clot presents clinical challenges in handling and securing the fibrin clot to the meniscal body to obtain a sufficiently long time-of-residence. Rode, S.A., "Arthroscopic meniscal repair with use of the outside-in technique," *Instr Course Lect*, 49, pp 195-206 (2000).

[0012] With meniscal allografts, there is a risk of disease transfer, poor revascularization, and infiltration and breaking down by host cells resulting in joint instability. In addition, the new tissue replacing the allograft may not be of sufficient quality to restore normal function. See: Sweigart, M.A. and K.A. Athanasiou, "Toward tissue engineering of the knee meniscus," *Tissue Eng.*, 7(2) pp 111-29 (2001); Boss, A., J. Klimkiewicz and F. H. Fu, "Technical innovation: creation of a peripheral vascularized trough to enhance healing in cryopreserved meniscal allograft reconstruction," *Knee Surg Sports Traumatol Arthrosc*, 8(3): pp 159-62 (2000); Siegel, M.G. and C.S. Roberts, "Meniscal allografts," *Clin Sports Med*, 12(1): pp 59-80 (1993).

[0013] Other meniscal implants may be difficult to handle during surgery and fixation or have insufficient mechanical properties for a sufficient time-of-residence *in vivo*.

[0014] It is also known to use naturally occurring extracellular matrices (ECMs) to provide a scaffold for tissue repair and regeneration. One such ECM is small intestine submucosa (SIS). SIS has been described as a natural biomaterial used to repair, support, and stabilize a wide variety of anatomical defects and traumatic injuries. The SIS material is derived from porcine small intestinal submucosa that models the qualities of its host when implanted in human soft tissues. Further, it is taught that the SIS material provides a natural matrix with a three-dimensional structure and biochemical composition that attracts host cells and supports tissue remodelling. SIS products, such as those sold under the trade marks OASIS and SURGISIS are available from Cook Biotech Inc.

[0015] Another SIS product which is sold under the trade mark RESTORE is available from DePuy Orthopaedics, Inc. The DePuy product is described for use during rotator cuff surgery, and is provided as a resorbable framework that allows the rotator cuff tendon to regenerate. The RESTORE implant is derived from porcine small intestine submucosa, a naturally occurring

ECM composed primarily of collagenous proteins, that has been cleaned, disinfected, and sterilized. Other biological molecules, such as growth factors, glycosaminoglycans, etc., have also been identified in SIS. See: Hodde et al., *Tissue Eng.*, 2(3): 209-217 (1996); Voytik-Harbin et al., *J. Cell. Biochem.*, 67: 478-491 (1997); McPherson and Badylak, *Tissue Eng.*, 4(1): 75-83 (1998); Hodde et al., *Endothelium* 8(1): 11-24; Hodde and Hiles, *Wounds*, 13(5): 195-201 (2001); Hurst and Bonner, *J. Biomater. Sci. Polym. Ed.*, 12(11): 1267-1279 (2001); Hodde et al., *Biomaterial*, 23(8): 1841-1848 (2002); and Hodde, *Tissue Eng.*, 8(2): 295-308 (2002). During nine years of preclinical testing in animals, there were no incidences of infection transmission from the implant to the host, and the RESTORE implant has not adversely affected the systemic activity of the immune system. See: Allman et al., *Transplant*, 17(11): 1631-1640 (2001); Allman et al., *Tissue Eng.*, 8(1):53-62 (2002).

[0016] While small intestine submucosa is available, other sources of submucosa are known to be effective for tissue remodelling. These sources include, but are not limited to, stomach, bladder, alimentary, respiratory, and genital submucosa. In addition, liver basement membrane is known to be effective for tissue remodelling, for example as disclosed in US-6379710, US-6171344, US-6099567 and US-5554389. Further, while ECM is most often porcine derived, it is known that these various ECM materials can be derived from non-porcine sources, including bovine and ovine sources. Additionally, the ECM material may also include partial layers of the lamina propria, muscularis mucosa, stratum compactum, submucosal plexuses, and vascular submucosa and/or other tissue materials depending upon factors such as the source from which the ECM material was derived and the delamination procedure.

[0017] Documents which disclose the use of ECMs for the regeneration and repair of various tissues include US-6379710, US-6187039, US-6176880, US-6126686, US-6099567, US-6096347, US-5997575, US-5993844, US-5968096, US-5955110, US-5922028, US-5885619, US-5788625, US-5733337, US-5762966, US-5755791, US-5753267, US-5711969, US-5645860, US-5641518, US-5554389, US-5516533, US-5460962, US-5445833, US-5372821, US-5352463, US-5281422 and US-5275826.

[0018] In one aspect, the present invention provides an implantable tissue repair device comprising a cover and tissue regeneration material. The cover includes a top panel and a bottom panel joined together along a leading edge. The tissue regeneration material is positioned between the top and bottom panels. The cover includes a continuous sheet of biocompatible material extending across the edge and into the top panel and bottom panel. The cover is thicker along the leading edge than at least a portion of the top panel and thicker than at least a portion of the bottom panel. At least a portion of one of the panels covering the tissue regen-

eration material is thicker than a portion of the other panel covering the tissue regeneration material.

[0019] In another aspect, the present invention provides an implantable tissue repair device comprising a cover and tissue regeneration material. The cover includes a top panel and a bottom panel joined together along a leading edge. The cover includes a plurality of laminae of biocompatible material. Some of the laminae of the cover extend across the leading edge and into the top panel and bottom panel. The cover has more laminae along the leading edge than at least a portion of the top panel and has more laminae along the leading edge than at least a portion of the bottom panel; and at least a portion of one of the panels covering the tissue regeneration material has more laminae than a portion of the other panel.

[0020] In another aspect, the present invention provides an implantable tissue repair device comprising a cover and tissue regeneration material. The cover includes a top panel and a bottom panel joined together along a leading edge. The tissue regeneration material is positioned between the top and bottom panels. The tissue regeneration material has a first side and a second side. The cover includes an outer group of laminae of biocompatible material and an inner group of laminae of biocompatible material. The laminae of the inner group extend over the first side of the tissue regeneration material. The laminae of the outer group extend across the leading edge, over the laminae of the inner group and over the second side of the tissue regeneration material.

[0021] In another aspect, the present invention provides a method of making an implantable tissue repair device. The method comprises providing a mould having a cavity, a surface surrounding the cavity and a groove spaced from the cavity. A first sheet of biocompatible material is placed on the surface of the mould with part of the sheet filling the cavity and part of the sheet received in the groove. Tissue regeneration material is then placed on the portion of the first sheet in the cavity. The first sheet is then folded along the portion in the groove to cover the tissue regeneration material with the sheet.

[0022] In a further aspect, the invention provides an implantable tissue repair device comprising:

a cover including a top panel and a bottom panel joined together along a leading edge;
tissue regeneration material between the top and bottom panels;

wherein:

the cover includes a plurality of laminae of biocompatible material some of the laminae of the cover extend across the leading edge and into the top panel and bottom panel;
the cover has more laminae along the leading edge

than at least a portion of the top panel and has more laminae along the leading edge than at least a portion of the bottom panel; and
at least a portion of one of the panels covering the tissue regeneration material has more laminae than a portion of the other panel.

[0023] In yet another aspect, the invention provides an implantable tissue repair device comprising:

a cover including a top panel and a bottom panel joined together along a leading edge;
tissue regeneration material between the top and bottom panels, the tissue regeneration material having a first side and a second side;

wherein:

the cover includes an outer group of laminae of biocompatible material and an inner group of laminae of biocompatible material;
the laminae of the inner group extend over the first side of the tissue regeneration material;
the laminae of the outer group extend across the leading edge, over the laminae of the inner group and over the second side of the tissue regeneration material.

[0024] A method of making an implantable tissue repair device includes providing a mould having a cavity and a surface surrounding the cavity. A first sheet of biocompatible material is placed on the surface of the mould. Part of the sheet is received in the cavity. Tissue regeneration material is placed on the portion of the first sheet in the cavity. A second sheet of biocompatible material is placed over the tissue regeneration material. The first sheet is then folded over the second sheet.

[0025] In another aspect, the invention provides a method of making an implantable tissue repair device comprising:

providing a mould having a cavity and a surface surrounding the cavity;
placing a first sheet of biocompatible material on the surface of the mould with part of the sheet received in the cavity;
placing tissue regeneration material on the portion of the first sheet in the cavity;
placing a second sheet of biocompatible material over the tissue regeneration material; and
folding the first sheet over the second sheet.

[0026] Embodiments of the invention will now be described by way of example with reference to the accompanying drawings, in which:

FIG. 1 is a perspective view of a tissue repair device or implant incorporating the principles of the present

invention, showing the top surface of the implant;
FIG. 2 is a perspective view of the tissue repair device or implant of FIG. 1 showing the bottom surface of the implant;

FIG. 3 is a top plan view of the tissue repair device or implant of FIGS. 1-2;

FIG. 4 is a bottom plan view of the tissue repair device or implant of FIGS. 1-3;

FIG. 5 is a side view of the tissue repair device or implant of FIGS. 1-4;

FIG. 6 is a top plan view of one type of tissue regeneration material that may be used in the tissue repair device or implant of the present invention;

FIG. 7 is a side view of the tissue regeneration material of FIG. 6;

FIG. 8 is a diagrammatic representation of the tissue repair device or implant of FIGS. 1-5, with the wings removed and the device implanted at a defect site in a meniscus;

FIG. 8A is a diagrammatic representation of the tissue repair device or implant of FIGS. 1-5, implanted at a defect site near the posterior horn of the meniscus, with one of the wings of the device removed and the other wing secured to the patient's tibia;

FIG. 9 is an enlarged cross-sectional view of the tissue repair device or implant of FIGS. 1-5, taken along line 9-9 of FIG. 3;

FIG. 10 is a top plan view of an apparatus for making the tissue repair device or implant of FIGS. 1-5 and 9;

FIG. 11 is a cross-section of the device taken along line 11-11 of FIG. 10;

FIG. 12 is a cross-section of the mould of FIGS. 10-11, taken along line 12-12 of FIG. 10;

FIG. 13 is an enlarged cross-section of a portion of the mould of FIGS. 10-12, showing one stage of the manufacturing process;

FIG. 14 is an enlarged cross-section of a portion of the mould of FIGS. 10-12, showing a later stage of the manufacturing process;

FIG. 15 is an enlarged cross-section of a portion of the mould of FIGS. 10-12 showing a later stage of the manufacturing process; and

FIG. 16 is an enlarged cross-section of a portion of the mould of FIGS. 10-12 showing a later stage of the manufacturing process.

[0027] Referring to the drawings, FIGS. 1-5, 8-9 and 16 show a tissue repair device or implant 10 in the form of a cartilage repair device, especially a meniscal repair device. However, it should be understood that the principles of the present invention may be applied to other repair devices, such as those designed to be implanted to repair defects in fibrocartilage other than the meniscus.

[0028] As shown in FIG. 9, the illustrated tissue repair device or implant 10 comprises a cover 12 and a mass of tissue regeneration material 14. In the illustrated tis-

sue repair device or implant 10, the mass of tissue regeneration material 14 is enclosed within the cover 12. The illustrated mass of tissue regeneration material 14 is wedge shaped, with an apex 15. It should be understood that the present invention is not limited to such a wedge-shaped device unless expressly called for in the claims. The shape of the space where the implant will be implanted primarily dictates the shape of the implant. For example, if the defect space has a circular shape with a certain depth, the principles of the present invention can be used to make an implant appropriate for that application.

[0029] As shown in FIGS. 1-5 and 9, the cover 12 comprises a top portion or panel 16, a bottom portion or panel 18, and three side portions 20, 22, 24. All of the portions 16, 18, 20, 22, 24 are integral in the illustrated embodiment. The cover 12 also has a fold line 26 along its leading edge, substantially at the apex 15 of the wedge of tissue regeneration material 14. As shown in FIGS. 5 and 9, the cover is substantially flat along the leading edge 26, and the top panel 16 is parallel to the bottom panel 18. At the tissue regeneration material 14, the top panel 16 diverges from the bottom panel 18 at an angle α shown in FIG. 5. In the illustrated embodiment, the angle α is about 30°, but it should be understood that the invention is not limited to any particular angular relationship between the panels unless expressly called for in the claims.

[0030] In the illustrated embodiment, the tissue repair device 10 also includes a pair of outwardly-extending tabs or wings 23, 25. These tabs or wings 23, 25 comprise integral extensions of the cover 12, and are provided for anchoring the tissue repair device 10 to native tissue such as native parts of the meniscus. FIG. 8 illustrates a tissue repair device of the present invention implanted in a meniscus 28, shown with sutures 30 affixing the device 10 to the native meniscus 28.

[0031] The cover 12 in the illustrated embodiment comprises a plurality of sheets of bioremodelable material affixed together. Generally, as shown in FIG. 9, there are two groups of sheet laminae: an outer group of laminae 32 and an inner group of laminae 34. The outer group of laminae 32 extend along the entire length of the top portion or panel 14, across the fold line 26 and along the entire length of the bottom portion or panel 16 of the cover 12. The outer group of laminae 32 also extend across the width of the cover 12. The inner group of laminae 34 extend only along the length and width of the top portion or panel 14 of the cover 12 to the fold line 26. As shown in FIG. 9, the inner group of laminae 34 are doubled over at the fold line 26 in the illustrated embodiment. However, it should be understood that some or all of the inner group of laminae 34 need not be doubled over, and could have edges underlying the outer laminae 32 at or near the leading edge 26 of the implant 10.

[0032] Thus, the outer group of laminae 32 cover the mass of tissue regeneration material 14. The top surface

36 of the mass of tissue regeneration material 14 is covered by the doubled-over inner group of laminae 34 and the outer group of laminae 32. The leading edge 26 of the implant comprises the doubled-over inner group of laminae 34 covered by the outer group of laminae 32. The part of the top portion or panel 16 overlying the top surface 36 of the mass of tissue regeneration material 14 is three times as thick as the part of the bottom portion or panel 18 covering the remainder of the mass of tissue regeneration material. The leading edge 26 and the trailing edge 38 of the implant 10 is four times as thick as the part of the bottom portion or panel 18 covering the mass of tissue regeneration material 14. The leading edge 26 presents no exposed edges of the individual laminae, while the edges of the laminae are exposed at the trailing edge 38 of the implant 10.

[0033] In the illustrated embodiment, the outer group of laminae 32 and inner group of laminae each comprises five layers of continuous sheets of biocompatible, bioremodelable material. Thus, the leading edge 26 and trailing edge each comprise twenty layers of continuous sheets of biocompatible, bioremodelable material. The part of the top portion or panel 16 overlying the mass of tissue regeneration material 14 comprises fifteen layers of continuous biocompatible, bioremodelable material. The part of the bottom portion or panel 18 covering the remainder of the mass of tissue regeneration material 14 comprises five layers of biocompatible, bioremodelable material. It should be understood that these numbers of layers are provided as examples only; fewer or more layers could be used for either the outer group of laminae 32 or the inner group of laminae 34. Individual layers are indicated at 32A-32E and 34A-34E in FIG. 9. It should be understood that for clarity of illustration, FIG. 9 illustrates the individual layers on only portions of the cover.

[0034] In the illustrated embodiment, each layer 32A-32E and 34A-34E comprises a sheets of small intestine submucosa (SIS). Each layer forming the outer group of laminae 32 and inner group of laminae 34 could also or alternatively comprise a biocompatible polymer, or a bioremodelable collagenous tissue matrix, such as another naturally occurring extracellular matrix material, all as defined below. Each group of laminae 32, 34 could comprise a homogeneous laminate, or could comprise layers of different materials. For example, a hybrid structure like that disclosed in US-A-2003/0023316 could be used. The groups of laminae 32, 34 could comprise such materials alone or together with bioactive agents, biologically derived agents, cells, a biological lubricant or a biocompatible inorganic material, as defined below.

[0035] "Biocompatible polymers" is intended to include both synthetic polymers and biopolymers (e.g., collagen). Examples of biocompatible polymers include: polyesters of [alpha]-hydroxycarboxylic acids, such as poly(L-lactide) (PLLA), polyglycolide (PGA), self-reinforced PLLA and self-reinforced PGA; poly-p-dioxanone (abbreviated as PDO or PDS); polyhydroxyacids, poly

(ortho esters); poly(beta-hydroxybutyrate) (PHB); poly (PHB-hydroxyvaleric acid), pseudo-poly(aminoacids) or polyiminocarbonates; poly(glycolide-co-trimethylene carbonate); polycaprolactone (PCL); polyvinyl alcohol (PVA); polyethylene oxide (PEO); polymers disclosed in US-6333029 and US-6355699; and any other bioresorbable and biocompatible polymer, co-polymer or mixture of polymers or copolymers that are utilized in the construction of prosthetic implants (e.g. 85:15 PLLA: PGA, 90:10 PGA:PLLA, or any polymer or co-polymer listed above in combination with a nondegradable material, or any combination of the above at any co-polymer ratio.) In addition, as new biocompatible, bioresorbable materials are developed, it is expected that at least some of them will be useful materials from which orthopaedic devices may be made. It should be understood that the above materials are identified by way of example only, and the present invention is not limited to any particular material unless expressly called for in the claims.

[0036] "Bioremodelable collagenous tissue matrix" is intended to include matrices derived from native tissue selected from the group consisting of skin, artery, vein, pericardium, heart valve, dura mater, ligament, bone, cartilage, bladder, liver, stomach, fascia and intestine, tendon, whatever the source. Although "naturally occurring bioremodelable collagenous tissue matrix" is intended to refer to matrix material that has been cleaned, processed, sterilized, and optionally crosslinked, it is not within the definition of a naturally occurring bioremodelable collagenous tissue matrix to purify the natural fibres and reform a matrix material from purified natural fibres. The term "bioremodelable collagenous tissue matrices" includes "extracellular matrices" within its definition.

[0037] "Naturally-occurring extracellular matrix material(s)" or "ECM" refers to collagen scaffolds for tissue repair and regeneration that have been derived from vertebrate tissue. One such ECM material that may be used for cartilage regeneration is submucosa, and small intestine submucosa (SIS) in particular. As used herein, "SIS" is intended to include small intestine submucosa unless otherwise limited. Moreover, as used herein, "ECM" is intended to include all SIS, as well as materials made from the other sources of submucosa (e.g. bladder, stomach and liver tissue from bovine, ovine and porcine sources) and materials derived from liver basement membrane (from whatever source) unless otherwise limited. For the purposes of this invention, it is within the definition of a naturally occurring ECM to clean, delaminate, and/or comminute the ECM, to cross-link the collagen within the ECM, and to form a foam or other structure from the ECM. It is also within the definition of naturally occurring ECM to fully or partially remove one or more components or subcomponents of the naturally occurring matrix. However, it is not within the definition of a naturally occurring ECM to extract or separate and purify the natural components or subcomponents (e.g.

collagen or growth factor) and reform a matrix material from these extracted and purified components or sub-components. Also, while reference is made to SIS, it is understood that other naturally occurring ECMs such as stomach, bladder, alimentary, respiratory, and genital submucosa, and liver basement membrane, for example, whatever the source (e.g. bovine, porcine, ovine, etc) can be used in accordance with this invention. Thus, in this application, the terms "naturally occurring extracellular matrix" or "naturally occurring ECM" are intended to refer to extracellular matrix material that has been cleaned, disinfected, sterilized, and optionally cross-linked.

[0038] "Bioactive agents" include one or more of the following: chemotactic agents; therapeutic agents (e.g., antibiotics, antimicrobials, steroidal and non-steroidal analgesics and anti-inflammatories, anti-rejection agents such as immunosuppressants and anti-cancer drugs); various proteins (e.g., short chain peptides, active or inactive peptides, bone morphogenic proteins, glycoproteins and lipoproteins); cell attachment mediators; biologically active ligands; integrin binding sequence; ligands; various growth and/or differentiation agents (e.g., epidermal growth factor, IGF-I, IGF-II, TGF- β I-III, growth and differentiation factors, vascular endothelial growth factors, fibroblast growth factors, platelet derived growth factors, insulin-like growth factor and transforming growth factors, parathyroid hormone, parathyroid hormone related peptide, bFGF; TGF β superfamily factors; bone morphogenetic proteins; BMP-2; BMP-4; BMP-6; BMP-12; sonic hedgehog; GDF5 (also known as BMP-14 or MP-52 or CDMP-1); GDF6; GDF8; CDMP-2; CDMP-3; PDGF); small molecules or protein equivalents that affect the upregulation of specific growth factors or other processes occurring during a healing response (e.g. TP508 and that sold under the trade mark Chrysalin, both available from OrthoLogic, Tempe, Arizona); tenascin-C; hyaluronic acid; chondroitin sulfate; fibronectin; decorin; thromboelastin; thrombin-derived peptides; heparin-binding domains; heparin; heparan sulfate; DNA fragments and DNA plasmids as sole constituents or when incorporated into appropriate vectors, such as viral constructs. If other such substances have therapeutic value in the orthopaedic field, it is anticipated that at least some of these substances will have use in the present invention, and such substances should be included in the meaning of "bioactive agent" and "bioactive agents" unless expressly limited otherwise.

[0039] "Biologically derived agents" include one or more of the following: bone (autograft, allograft, and xenograft) and derivatives of bone; cartilage (autograft, allograft and xenograft), including, for example, meniscal tissue, and derivatives; ligament (autograft, allograft and xenograft) and derivatives; derivatives of intestinal tissue (autograft, allograft and xenograft), including for example submucosa; derivatives of stomach tissue (autograft, allograft and xenograft), including for exam-

ple submucosa; derivatives of bladder tissue (autograft, allograft and xenograft), including for example submucosa; derivatives of alimentary tissue (autograft, allograft and xenograft), including for example submucosa; derivatives of respiratory tissue (autograft, allograft and xenograft), including for example submucosa; derivatives of genital tissue (autograft, allograft and xenograft), including for example submucosa; derivatives of liver tissue (autograft, allograft and xenograft), including for example liver basement membrane; derivatives of skin (autograft, allograft and xenograft); platelet rich plasma (PRP), platelet poor plasma, bone marrow aspirate, demineralized bone matrix, insulin-like-growth factor, whole blood, fibrin and blood clot. Purified ECM and other collagen sources are also intended to be included within "biologically derived agents." If other such substances have therapeutic value in the orthopaedic field, it is anticipated that at least some of these substances will have use in the present invention, and such substances should be included in the meaning of "biologically-derived agent" and "biologically-derived agents" unless expressly limited otherwise. It should be understood that the above agents are identified by way of example only, and the present invention is not limited to any particular agent unless expressly called for in the claims.

[0040] "Cells" include one or more of the following: any connective tissue cells; chondrocytes; fibrochondrocytes or any cells from fibrocartilage tissues such as meniscus and intervertebral disks (specifically the annulus fibrosus); osteocytes; osteoblasts; osteoclasts; synoviocytes; fibroblasts (including fibroblasts originating from ligaments, tendons, skin, or other tissues); bone marrow cells; mesenchymal cells; stromal cells; stem cells; embryonic stem cells; precursor cells derived from adipose tissue; peripheral blood progenitor cells; stem cells isolated from adult, adolescent, neonatal, or fetal tissues; genetically transformed cells; a combination of any connective tissue cell type and other cells; a combination of chondrocytes and other cells; a combination of fibrochondrocytes and other cells; a combination of osteocytes and other cells; a combination of synoviocytes and other cells; a combination of fibroblasts and other cells; a combination of bone marrow cells and other cells; a combination of mesenchymal cells and other cells; a combination of stromal cells and other cells; a combination of stem cells and other cells; a combination of embryonic stem cells and other cells; a combination of precursor cells isolated from adult tissue and other cells; a combination of peripheral blood progenitor cells and other cells; a combination of stem cells isolated from adult, adolescent, neo-natal, or fetal tissues and other cells; and a combination of genetically transformed cells and other cells. If other cells are found to have therapeutic value in the orthopaedic field, it is anticipated that at least some of these cells will have use in the present invention, and such cells should be included within the meaning of "cell" and "cells" unless

expressly limited otherwise. Illustratively, in one example of embodiments that are to be seeded with living cells such as chondrocytes, a sterilized implant may be subsequently seeded with living cells and packaged in an appropriate medium for the cell type used. For example, a cell culture medium comprising Dulbecco's Modified Eagles Medium (DMEM) can be used with standard additives such as non-essential amino acids, glucose, ascorbic acid, sodium pyruvate, fungicides, antibiotics, etc., in concentrations deemed appropriate for cell type, shipping conditions, etc.

[0041] "Biological lubricants" include: hyaluronic acid and its salts, such as sodium hyaluronate; glycosaminoglycans such as dermatan sulfate, heparan sulfate, chondroitin sulfate and keratan sulfate; synovial fluid and components of synovial fluid, including as mucinous glycoproteins (e. g. lubricin), vitronectin, tribonectins, articular cartilage superficial zone proteins, surface-active phospholipids, lubricating glycoproteins I, II; and rooster comb hyaluronate. "Biological lubricant" is also intended to include commercial products such as the high molecular weight sodium hyaluronates sold by Bio-Technology General (Israel) Ltd of Rehovot, Israel under the trade mark ARTHREASE, and by Biomatrix, Inc of Ridgefield, N.J. (and distributed by Wyeth-Ayerst Pharmaceuticals of Philadelphia, Pa) under the trade mark SYNVISC Hylan G-F 20, and sodium hyaluronates available from Sanofi-Synthelabo, Inc., of New York, N. Y. (and manufactured by FIDIA S.p.A., of Padua, Italy) under the trade mark HYLAPAN, and by Pharmacia Corporation of Peapack, N.J. under the trade mark HEALON, in concentrations of 1%, 1.4% and 2.3% (for ophthalmologic uses). If other such substances have therapeutic value in the orthopaedic field, it is anticipated that at least some of these substances will have use in the concepts of the present disclosure, and such substances should be included in the meaning of "biological lubricant" and "biological lubricants" unless expressly limited otherwise.

[0042] "Biocompatible inorganic material(s)" include materials such as hydroxyapatite, all calcium phosphates, alpha-tricalcium phosphate, beta-tricalcium phosphate, calcium carbonate, barium carbonate, calcium sulfate, barium sulfate, polymorphs of calcium phosphate, ceramic particles, and combinations of such materials. If other such substances have therapeutic value in the orthopaedic field, it is anticipated that at least some of these substances will have use in the concepts of the present disclosure, and such substances should be included in the meaning of "biocompatible inorganic material" and "biocompatible inorganic materials" unless expressly limited otherwise.

[0043] The cover 12 of the implant 10 may be hardened or toughened as disclosed in US-A-2003/0032961 and US-A-2003/0036797.

[0044] The cover 12 of the implant 10 could also include fixating members such as: a length of bioresorbable suture; a bioresorbable barbed dart; a bioresorbable

tack; a bioresorbable backstop; or a bioresorbable locking member, as described in US-A-2003/0078617.

[0045] The mass of tissue regeneration material 14 is illustrated in FIGS. 6 and 7. In the illustrated embodiment, the mass of tissue regeneration material 14 is wedge shaped, although it should be understood that tissue regeneration material having other shapes can be used. For example, as disclosed in US-A-2003/0036797, the mass of tissue regeneration material could comprise rolls of comminuted SIS.

[0046] In the illustrated embodiment, the mass of tissue regeneration material 14 comprises comminuted SIS material or SIS foam, as described in US-A-2003/0044444. The mass or plug of tissue regeneration material 14 may also or alternatively comprise comminuted and/or lyophilized naturally occurring ECM (e.g., SIS) with the desired porosity and material density. The material density and/or porosity of the mass or plug may be varied to control cell migration and proliferation. Additional examples of materials that are usable for the mass of tissue regeneration material include ECM (e.g., SIS) powder, ECM (e.g., SIS) fibers, ECM (e.g., SIS) threads, ECM (e.g., SIS) mesh, ECM (e.g., SIS) wovens, ECM (e.g., SIS) non-wovens, ECM (e.g., SIS) braided materials, ECM (e.g., SIS) solutions, ECM (e.g., SIS) gel, ECM (e.g., SIS) paste, ECM (e.g., SIS) foam, and combinations of such materials. For the powder, solutions, gel and paste forms of SIS, the material may be prepared as described in US-5352463. In addition, unless expressly limited by the claims, the mass of tissue regeneration material could also comprise bioremodelable collagenous tissue matrices, either alone or in combination with an ECM. Moreover, the mass of tissue regeneration material could comprise a hybrid of a biocompatible polymer with and ECM or bioremodelable collagenous tissue matrix, as disclosed in US-A-2003/0021827 and US-A-2003/0023316. It should be understood that separate reference in the above list to the forms of ECM should not be taken to imply that the listed references are exclusive; for example, ECM non-wovens, ECM threads and ECM foam may all include ECM fibres.

[0047] The mass of tissue regeneration material 14 may also include bioactive agents, biologically derived agents, cells, a biological lubricant or a biocompatible inorganic material, as defined above.

[0048] An apparatus 50 for making the illustrated tissue repair device or implant 10 is shown in FIGS. 10-12. The apparatus 50 comprises a mould 52, a vacuum fixture 54, a nipple fitting 56, a fixture post 58 and a fixture base 60. The mould 52 includes a cavity 62, an elongate groove 64 spaced from the cavity 62 and a plurality of air vents 66 across the surface of the mould. The air vents 66 extend through the thickness of the mould and communicate with a plenum 68 in the vacuum fixture 54. The nipple fitting 56 also communicates with the plenum 68. A suitable hose (not shown) and vacuum pump (not shown) are connected to the nipple fitting 56 to draw air

through the air vents 66, into the plenum 68 and out through the nipple fitting 56.

[0049] The mould cavity 62 is shaped to correspond generally with the shape of the mass of tissue regeneration material 14. As described in more detail below, the mould groove 64 is used to define the fold line or leading edge 26 of the implant 10.

[0050] The steps of making the implant 10 are illustrated in FIGS. 13-16. First, individual layers of thin, moist, flexible sheets of the cover material, such as SIS, are laid out on top of each other and partially laminated by hand pressure to form the outer group of laminae 32 into an outer laminate sheet. In the illustrated embodiment, five thin sheets of SIS are layered together to form the outer group 32 of laminae into the outer laminate sheet. This outer laminate sheet (that is, the outer group 32 of laminae) is then laid on the top surface of the mould 52. The outer laminate sheet comprising has an area generally great enough to cover the entire top surface of the mould 52. The vacuum pulls the outer laminate sheet against the surface of the mould and into the cavity 62. Part of the outer laminate sheet also lays in the groove 64. At the end of this step in the manufacturing process, the outer laminate sheet generally conforms to the shape of the top surface of the mould 52, as shown in FIG. 13.

[0051] Next, the mass of tissue regeneration material 14 is placed in the cavity 62 that is lined by the outer laminate, as shown in FIG. 14. The mass of tissue regeneration material can be pre-shaped or could comprise loose particles.

[0052] Next, individual layers of moist, flexible sheets of the cover material, such as SIS, are laid out on top of each other and partially laminated by hand pressure to form the inner group of laminae 34 into an inner laminate sheet. In the illustrated embodiment, five thin sheets of SIS are layered together to form the inner laminate sheet (that is, the inner group of laminae 34). This inner laminate sheet is then laid on top of the outer laminate sheet and the mass of tissue regeneration material 14 as shown in FIG. 15. The inner laminate sheet has an area generally great enough to cover the entire surface of the outer laminate sheet and the mass of tissue regeneration material 14. As the inner laminate sheet is laid flat on the mould 52, the vacuum pulls the inner laminate sheet against the surfaces of the outer laminate sheet and the mass of tissue regeneration material. Part of the inner laminate sheet lays in the groove 64 as well.

[0053] Next, the outer laminate sheet and inner laminate sheet are folded along the portions received in the groove 64, back over the mass of tissue regeneration material 14. As shown in FIG. 16, the result is a structure having the greatest number of layers or laminae of the cover material at the leading and trailing edges 26, 38.

[0054] The raw implant may then be high pressure laminated while in the mould 52 and dried while still in the mould 52 in a vacuum drying bed. This drying step may still leave the mass of tissue regeneration material

in a wet state. The semi-finished implant may then be lyophilized to dry the mass of tissue regeneration material. Finally, the cover may be trimmed to form the implant as shown in FIGS. 1-4. It is expected that standard disinfection and sterilization techniques may be used with the implants produced by this method.

[0055] It should be understood that the above-described method of making the implant is provided as an example only. The invention is not limited to any particular method unless expressly called for in the claims.

[0056] It is anticipated that several different sizes and shapes of implants 10 would be made available to account for differences in the amount of tissue removed in a meniscectomy. Accordingly, there would also be several different moulds provided to produce these different sizes of implants 10. Accordingly, there would also be several different cutting dyes provided to produce these different implants.

[0057] It should be understood that the above-described manufacturing process is provided as an example only. The present invention is not limited to this process unless expressly set forth in the claims.

[0058] To use the implant of the present invention, the surgeon would perform a partial meniscectomy to remove diseased or damaged meniscal tissue. The implant 10 would be hydrated and then delivered to the site of the defect and fixated to the native meniscal tissue using suture or other fixating mechanisms. Devices which might be used to deliver the implant 10 arthroscopically include those disclosed in US patent applications nos. 10/610287, 60/483804 and 10/742020.

[0059] If there is sufficient native meniscal tissue present, the wings 23, 25 may be cut off the implant 10 and the implant fixated as shown in FIG. 8. If insufficient native meniscal tissue is present, such as if the implant 10 is to be affixed near the posterior horn of the meniscus 28, one of the wings 23, 25 may be cut off and the other left. As shown in FIG. 8A, the surgeon can then use the remaining wing (25 in FIG. 8A) to fix the implant directly to the patient's tibia 70, for example by inserting a screw 72 through the wing 25 and into the tibia 70.

[0060] Use of the implant of the present invention may be accompanied by use of a biological lubricant, as disclosed in US-A-2003/0033021 and US-A-2003/0033022.

[0061] A tissue repair device or implant 10 made according to the above described process was tested as follows. The device was implanted in a meniscal defect of a goat knee. The goat knee and implant were placed in a test apparatus with the knee joint at about 135° of flexion. Axial compression of 31.67±13.57 kg (70±30 pounds) was applied as the knee was moved through 5° of flexion/extension and as the tibia was translated approximately 3.18 mm (0.125 inch) in the anterior/posterior direction. The test was conducted for 100,000 cycles at 2 Hz, with an intermittent phosphate buffered saline (PBS, pH 7.2) mist. At the end of the test, the implant lost only 6.9±1.3% of its dry weight. There were no in-

cidences of the implant delaminating at the leading edge 26; the only delamination that occurred was at the periphery of the implant. However, the implant did not fail because it was held together at the site of delamination by sutures.

[0062] Thus, the implant of the present invention is mechanically robust and should be capable of withstanding handling and hydration during implantation without undergoing delamination.

[0063] The shape of the implant could be modified for use in replacing resected tissue from other joints, such as intra-articular cartilage in the temporomandibular joint or between vertebrae.

Claims

1. An implantable tissue repair device comprising:

a cover including a top panel and a bottom panel joined together along a leading edge; tissue regeneration material between the top and bottom panels;

wherein:

the cover includes a continuous sheet of biocompatible material extending across the edge and into the top panel and bottom panel; the cover along the leading edge is thicker than at least a portion of the top panel and thicker than at least a portion of the bottom panel; and at least a portion of one of the panels covering the tissue regeneration material is thicker than a portion of the other panel.

2. The implantable tissue repair device of claim 1 wherein at least part of the top panel is parallel to at least part of the bottom panel along at least part of the leading edge.

3. The implantable tissue repair device of claim 1 wherein the top panel and bottom panel are joined together along a trailing edge

4. The implantable tissue repair device of claim 1 wherein at least one of the cover and the tissue regeneration material includes a naturally occurring extracellular matrix material.

5. The implantable tissue repair device of claim 4 wherein the cover includes sheets of small intestine submucosa.

6. The implantable tissue repair device of claim 5 wherein the tissue regeneration material includes comminuted small intestine submucosa.

7. The implantable tissue repair device of claim 1 wherein the leading edge comprises a fold line.

8. The implantable tissue repair device of claim 1 wherein the device is sized and shaped to be used as a mensical implant.

9. A method of making an implantable tissue repair device comprising:

providing a mould having a cavity, a surface surrounding the cavity and a groove spaced from the cavity;
placing a first sheet of biocompatible material on the surface of the mould with part of the sheet received in the cavity and part of the sheet received in the groove;
placing tissue regeneration material on the portion of the first sheet in the cavity; and
folding the first sheet along the portion in the groove to cover the tissue regeneration material with the sheet.

10. The method of claim 9 further comprising placing a second sheet of biocompatible material on top of the tissue regeneration material before folding the first sheet.

11. The method of claim 9 further comprising placing a second sheet of biocompatible material on top of the tissue regeneration material and extending over the first sheet of biocompatible material and into the groove, and wherein the folding step includes folding both the first and second sheets along the portions in the groove to cover the tissue regeneration material with both the first and second sheets so that two layers of the second sheet cover the tissue regeneration material.

12. The method of claim 9 wherein the first sheet of biocompatible material comprises a laminate.

13. The method of claim 11 wherein the second sheet of biocompatible material comprises a laminate.

FIG. 1

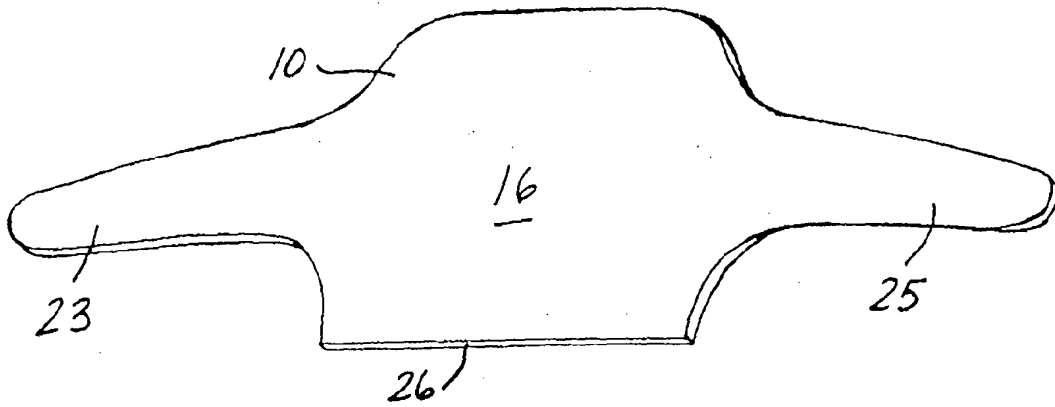


FIG. 2

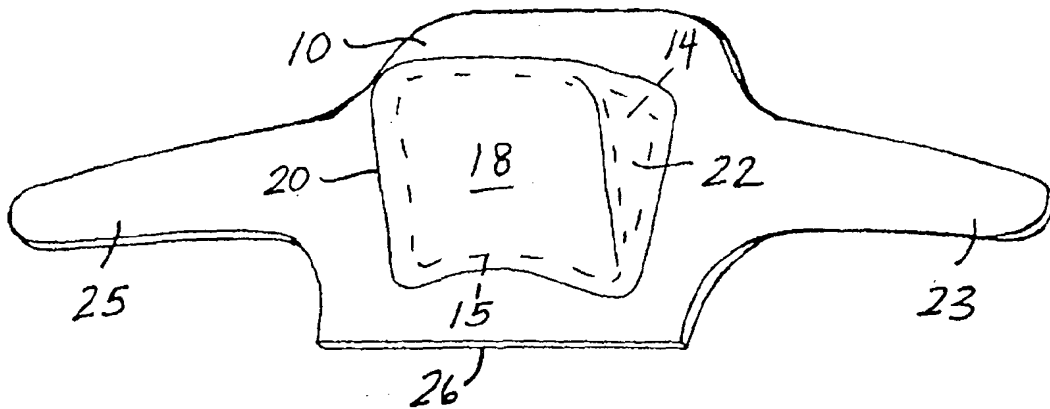
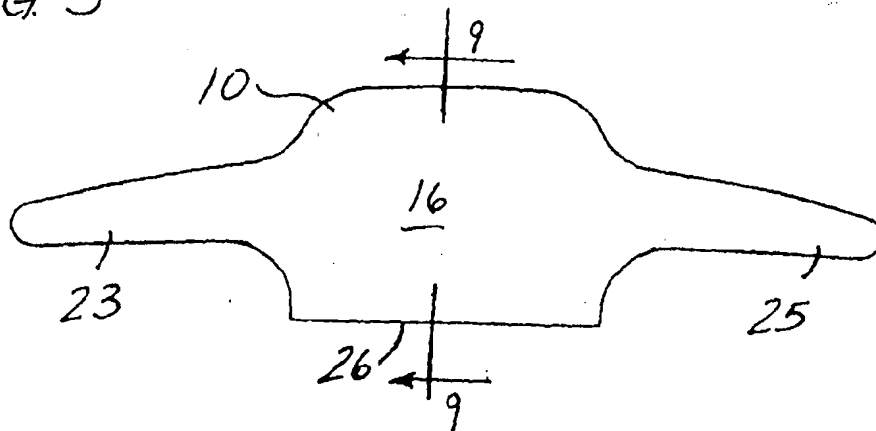


FIG. 3



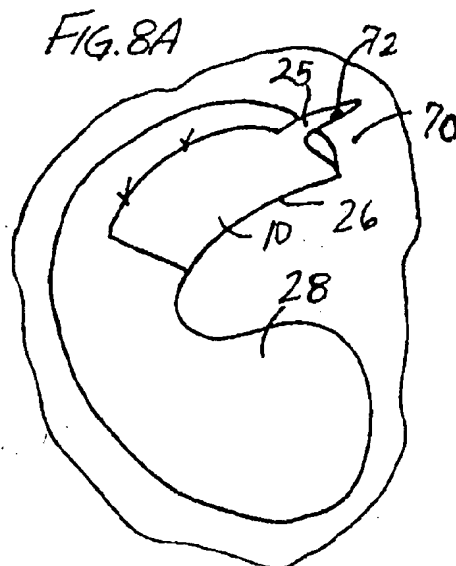
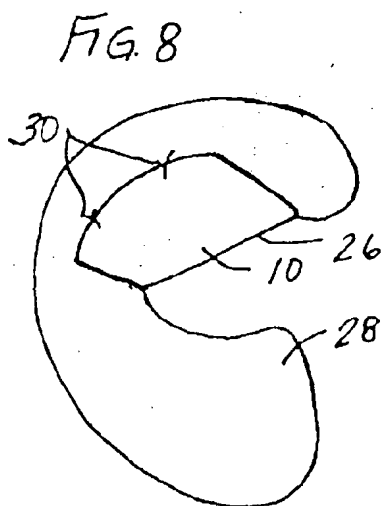
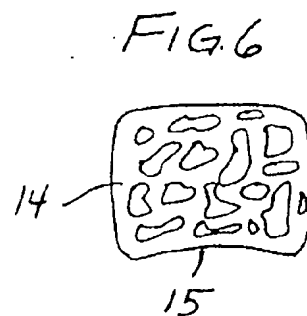
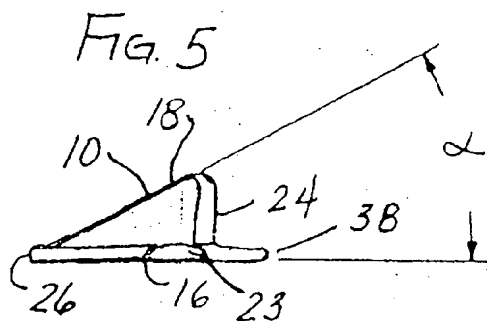
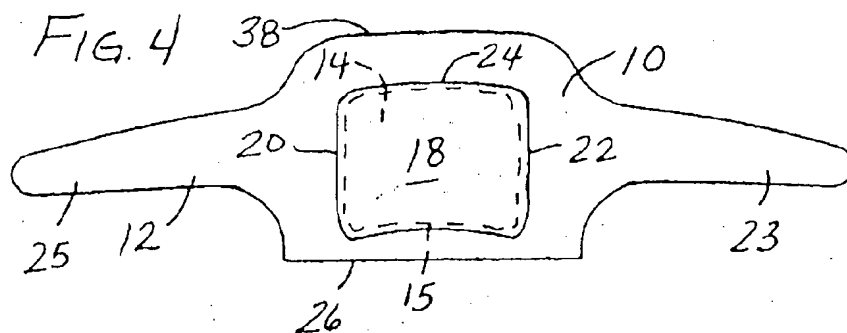


Fig 9

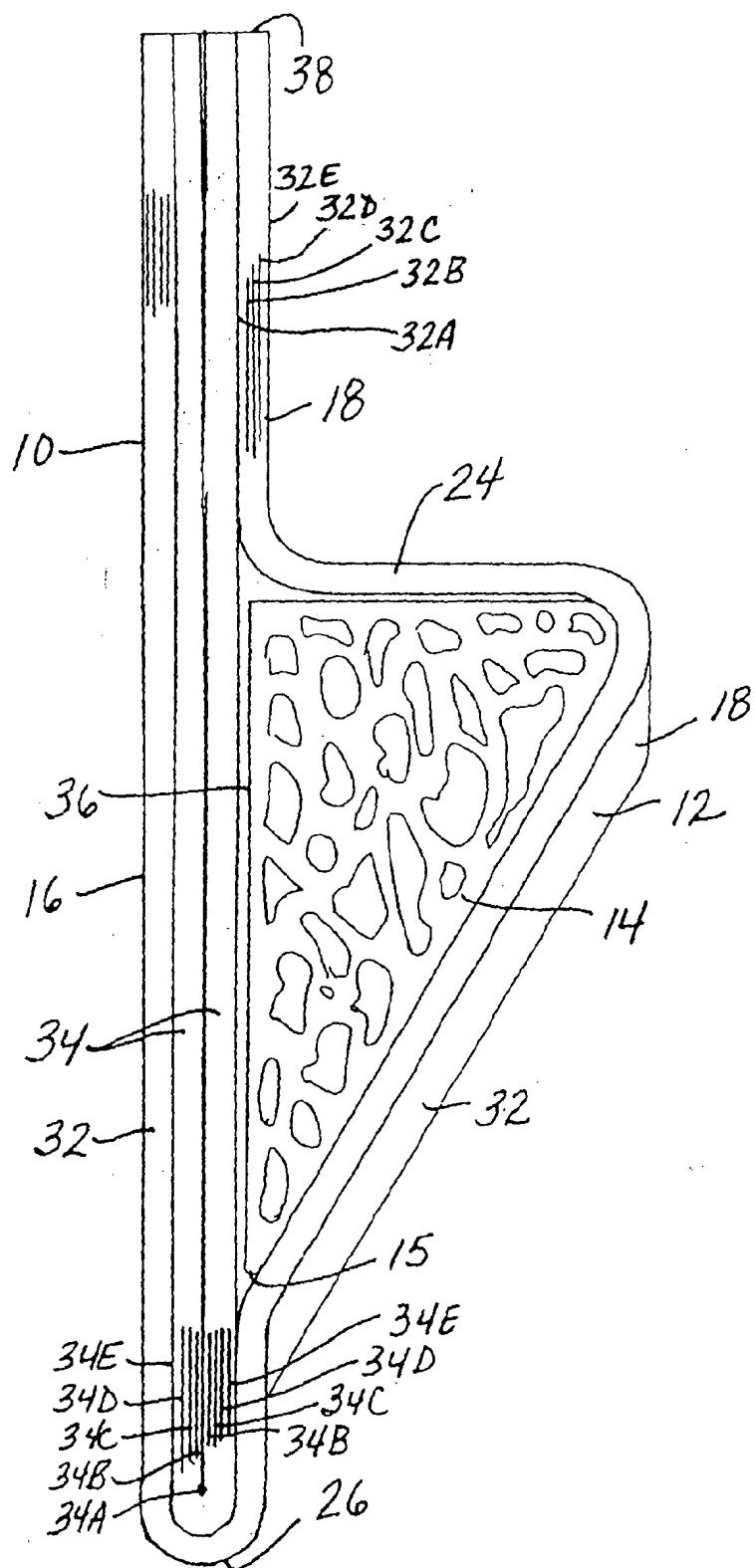


FIG 10

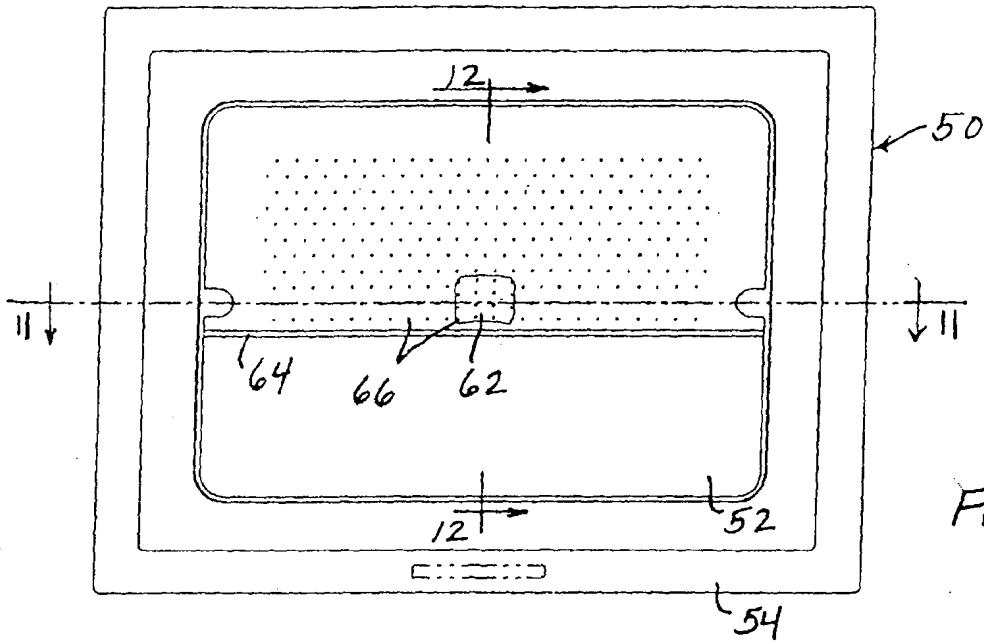


FIG. 12

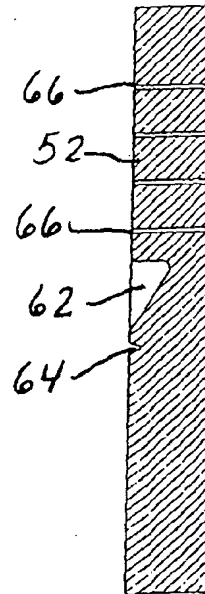


FIG. 11

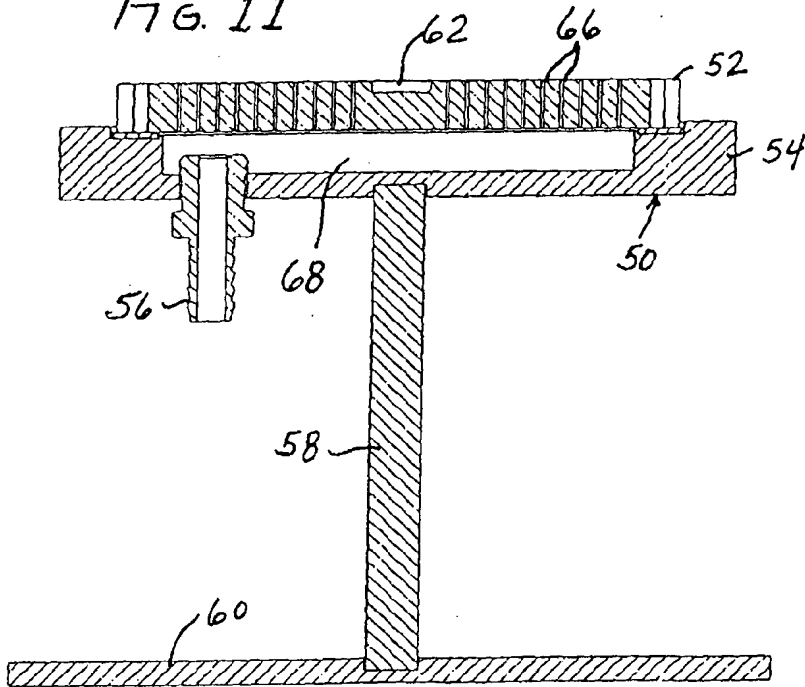


FIG 13

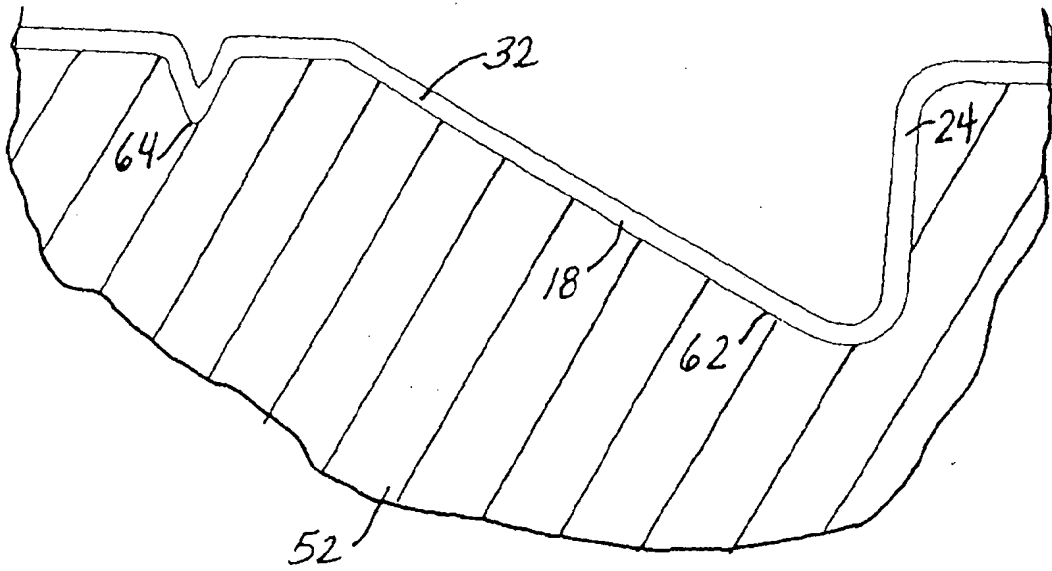


FIG. 14

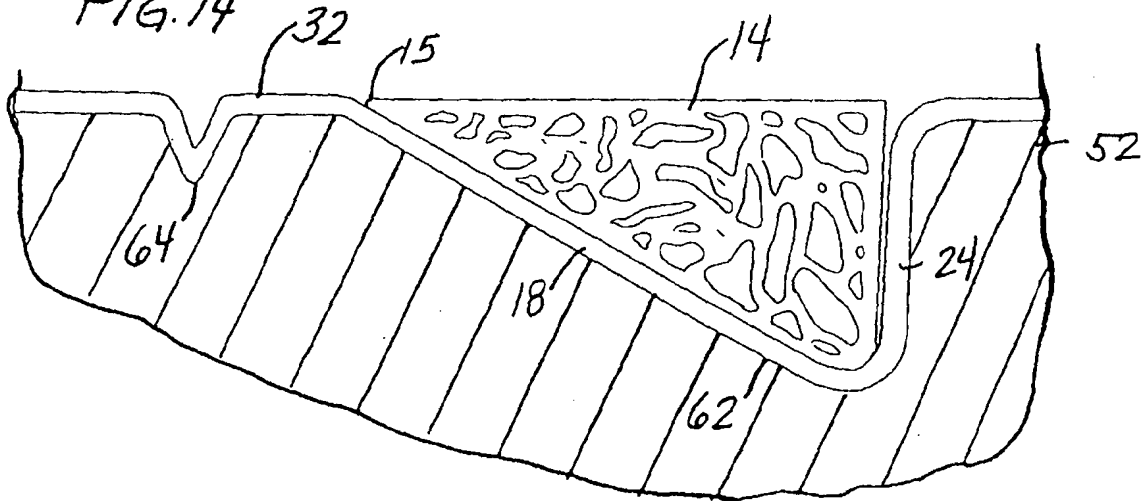


FIG. 15

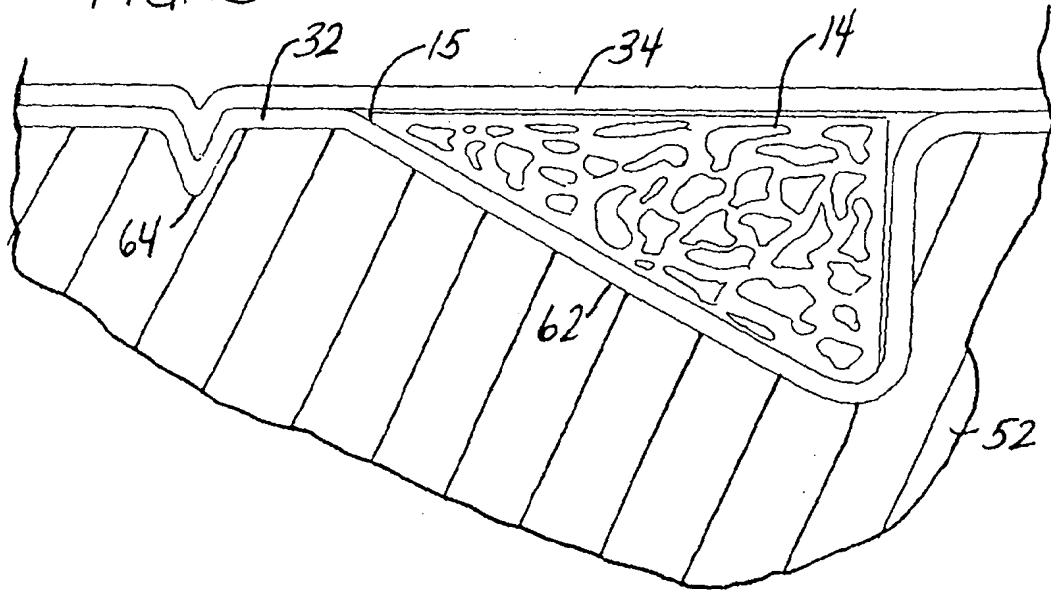
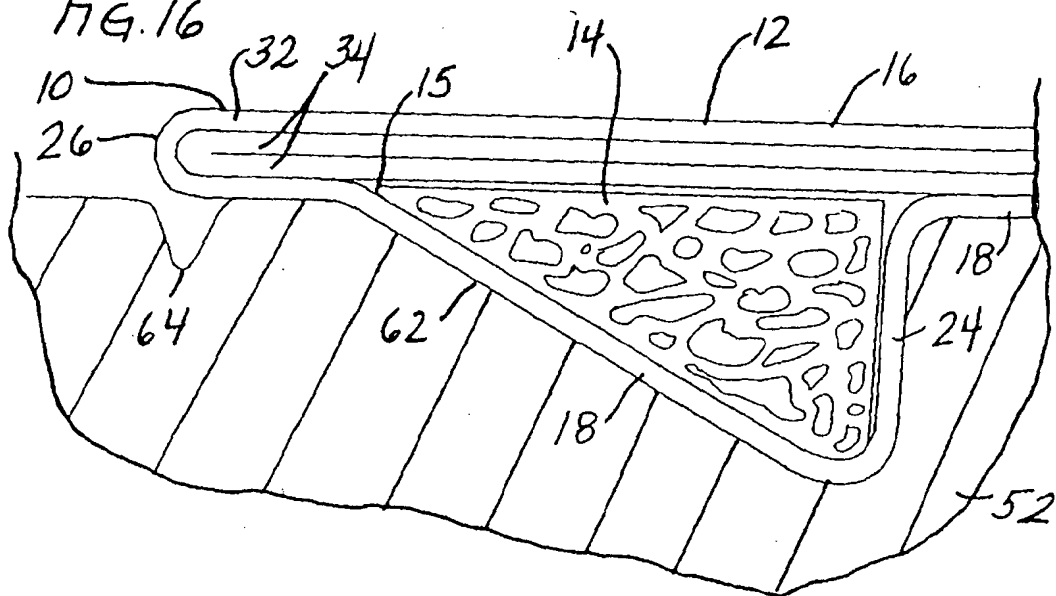


FIG. 16





European Patent
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EUROPEAN SEARCH REPORT

Application Number
EP 04 25 8075

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Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int.Cl.7)
X A	WO 03/007784 A (DEPUY PRODUCTS, INC.; MALAVIYA, PRASANNA; SCHWARTZ, HERBERT, EUGENE; WH) 30 January 2003 (2003-01-30) * page 27, line 18 - line 26 * * page 28, line 11 - page 30, line 5; figures 5,11 * -----	1-8 9-13	A61F2/00 A61F2/08 A61F2/28 A61F2/30 A61F2/38 A61B17/064
			TECHNICAL FIELDS SEARCHED (Int.Cl.7)
			A61F A61B
The present search report has been drawn up for all claims			
Place of search Berlin		Date of completion of the search 30 May 2005	Examiner Korth, C-F
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